

Principles and Applications of Brain-Computer Interfaces

Tzyy-Ping Jung

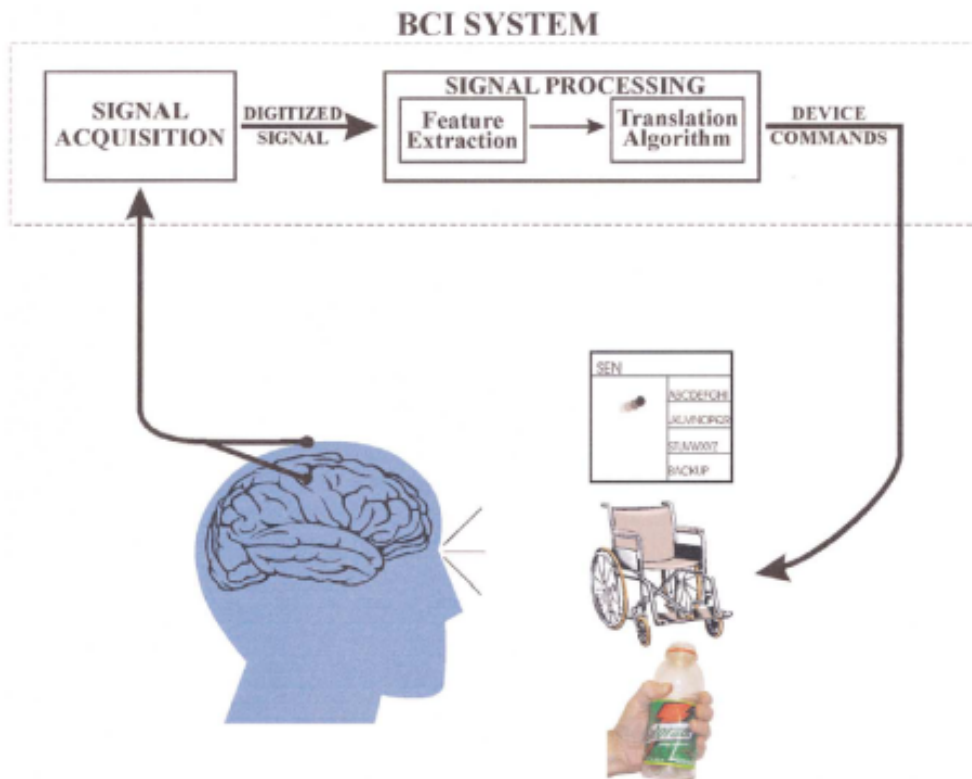
**Center for Advanced Neurological Engineering and
Swartz Center for Computational Neuroscience and
University of California San Diego, USA**

and

**Department of Computer Science
National Chiao-Tung University, Hsinchu, Taiwan**

- Working definitions of BCIs
- Types of BCIs
- Bio-signals for BCIs
- Typical EEG features used in BCIs
- Available tools
- Major components in BCIs
- Evaluations of BCI performance
- Application areas and examples
- Challenges in BCIs

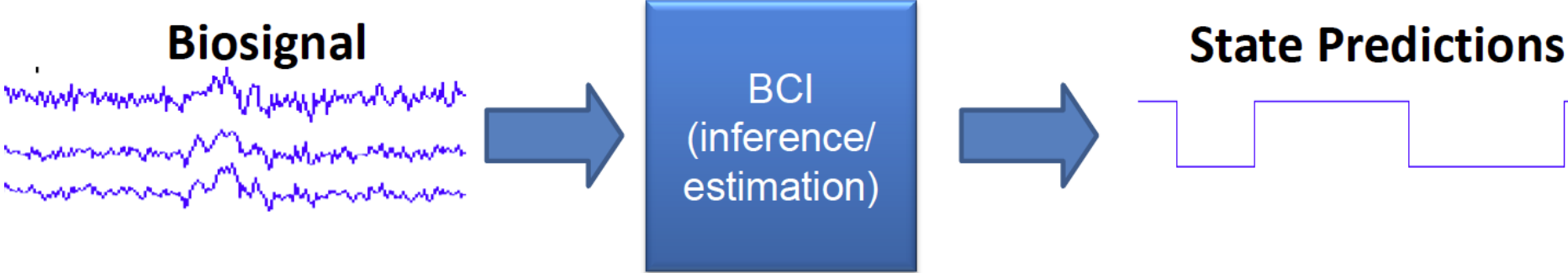
A **brain-computer interface (BCI)**, sometimes called a **direct neural interface** or a **brain-machine interface**, is a direct communication pathway between a brain and an external device. BCIs are often aimed at assisting, augmenting or repairing human cognitive or sensory-motor functions.



- **Direct:** The system must rely on direct measures of brain activity.
- **Real-time:** real-time refers to a maximum of a one minute delay between the user's formation of a relevant message or command and resulting feedback.
- **Feedback:** BCIs must present real-time feedback to the user. That is, the system must act on the user's intent so that the user can know whether s/he successfully conveyed the desired message or command.
- **Intentional:** The user must perform some voluntary, intentional, goal-directed mental activity each time s/he wishes to convey information. This criterion excludes all passive BCIs.

Our Working Definition of a BCI

A system which takes a biosignal measured from a person and predicts (in real time / on a single-trial basis) some abstract aspect of the person's neurological state, cognitive state, attention, or intention.



- **Active BCI (BMI):** a BCI derives its outputs from brain activity which is directly consciously controlled by the user, independently from external events, for controlling an application.
- **Reactive BCI:** a BCI derives its outputs from brain activity arising in reaction to external stimulation, which is indirectly modulated by the users for controlling an application.
- ***Passive or Affective BCI (BMI)*** derives its outputs from spontaneous brain activity without the purpose of voluntary control.

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- EEG or MEG



BioSemi B.V.



MINDO

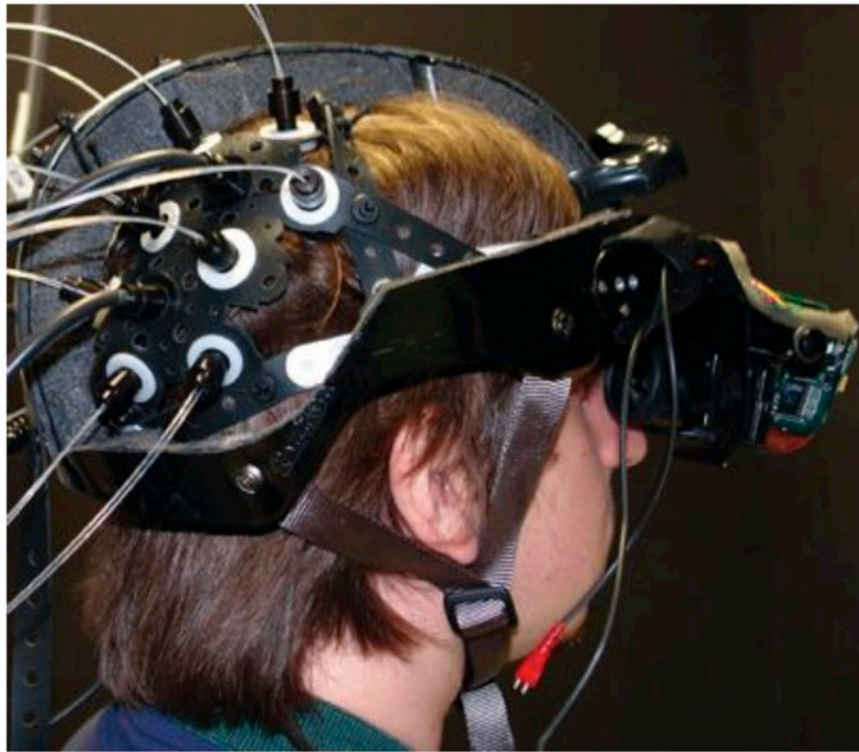


Cognionics, Inc



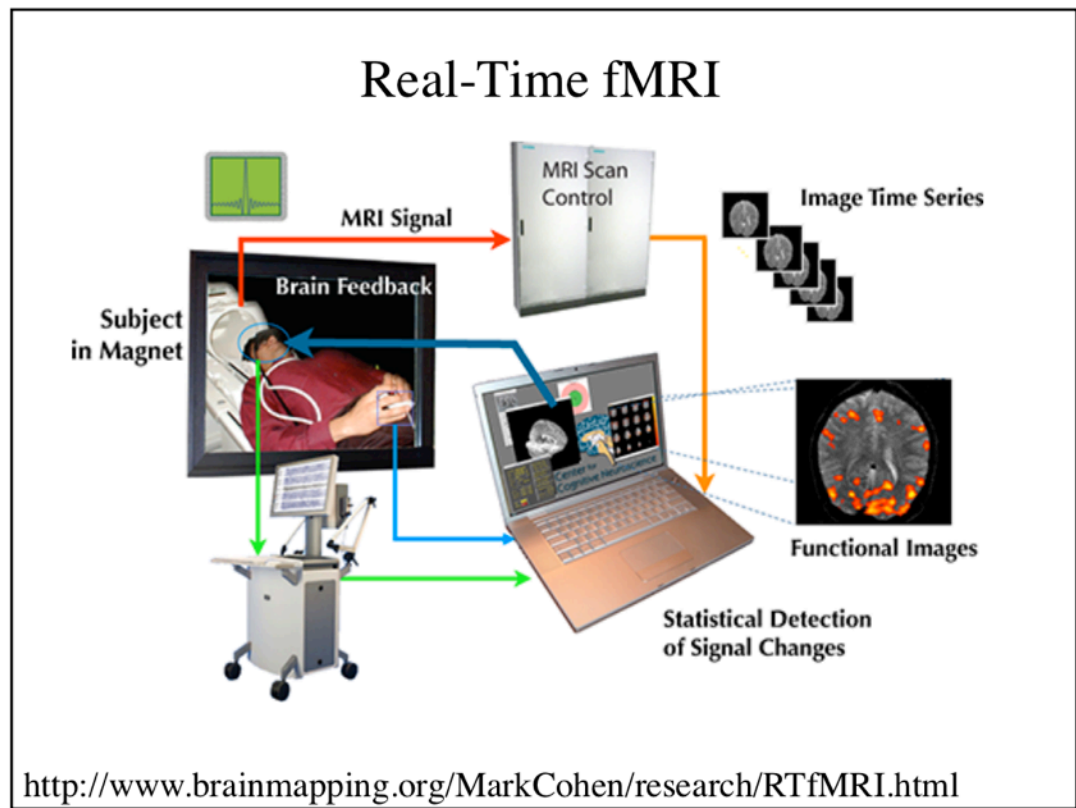
NIMH

- Functional Near-Infrared Spectroscopy (fNIRS)

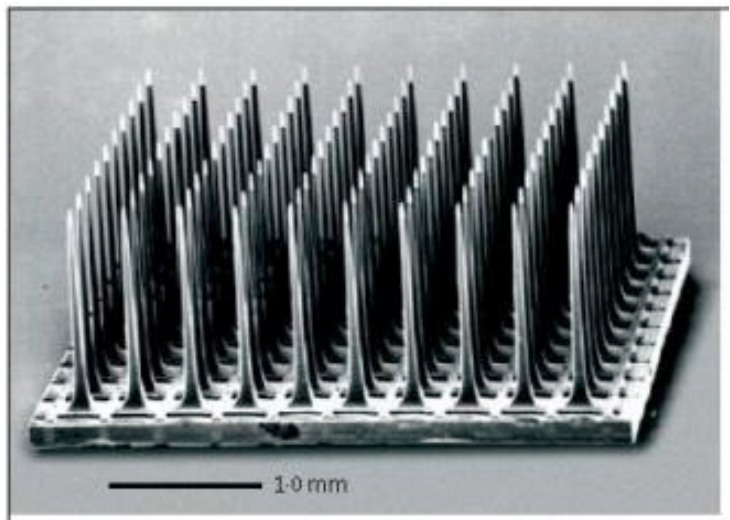


Seraglia et al., 2011

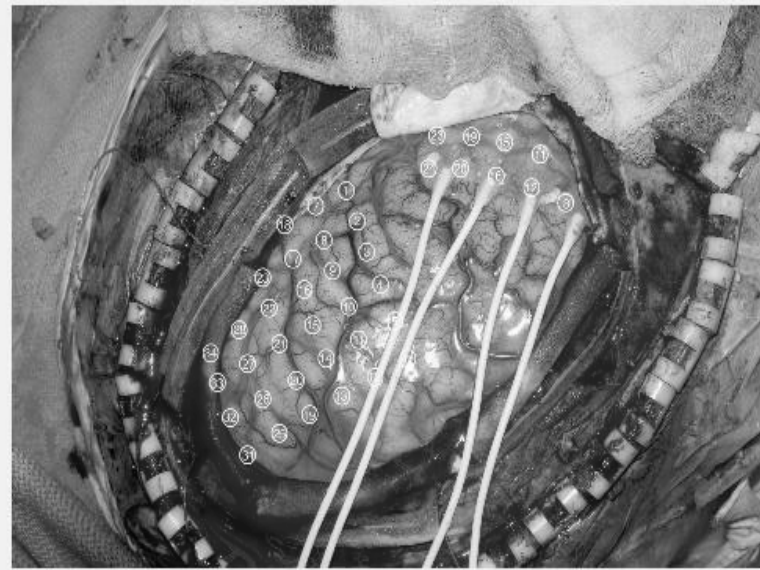
- fMRI



- Microarrays, ECoG, Neurochips, etc.



Utah Electrode

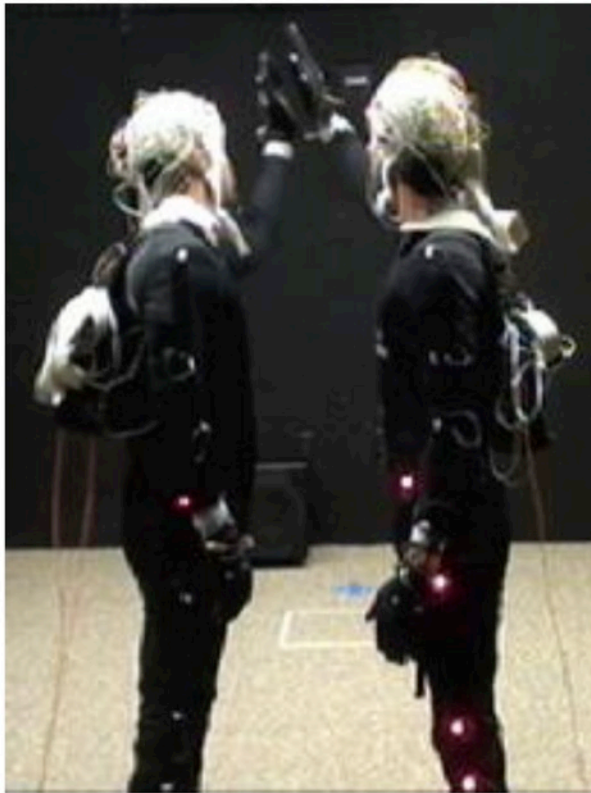


- Electromyography (EMG), Electrocardiography (ECG), Electrooculography (EOG)



Microsoft, Inc

- Motion capture, eye-tracking



SCCN MoBI Lab



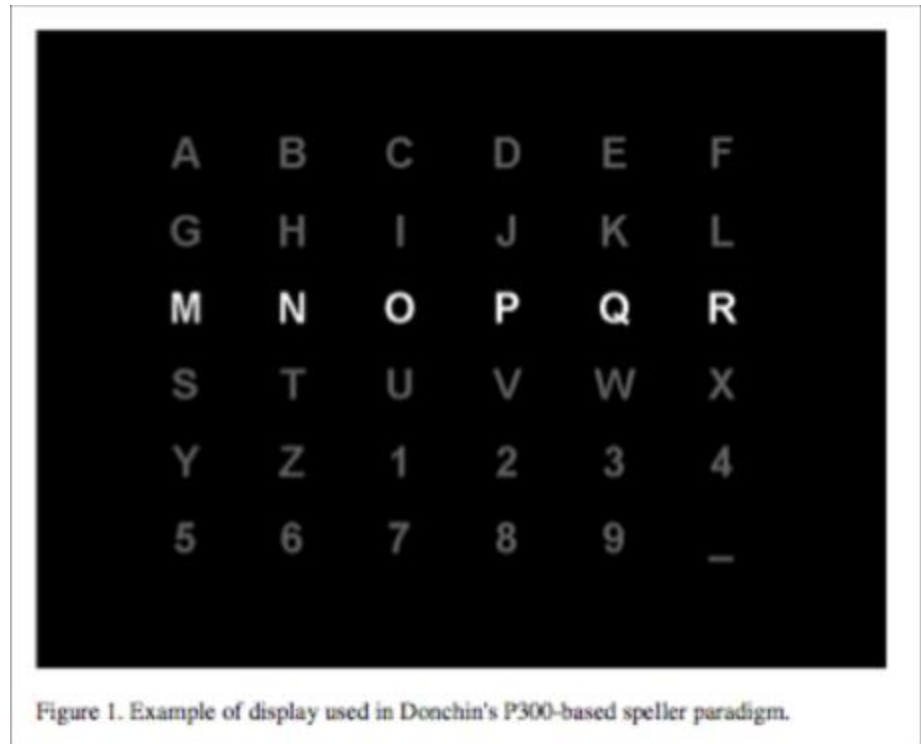
SensoMotoric Instruments
(EEG: Emotiv)

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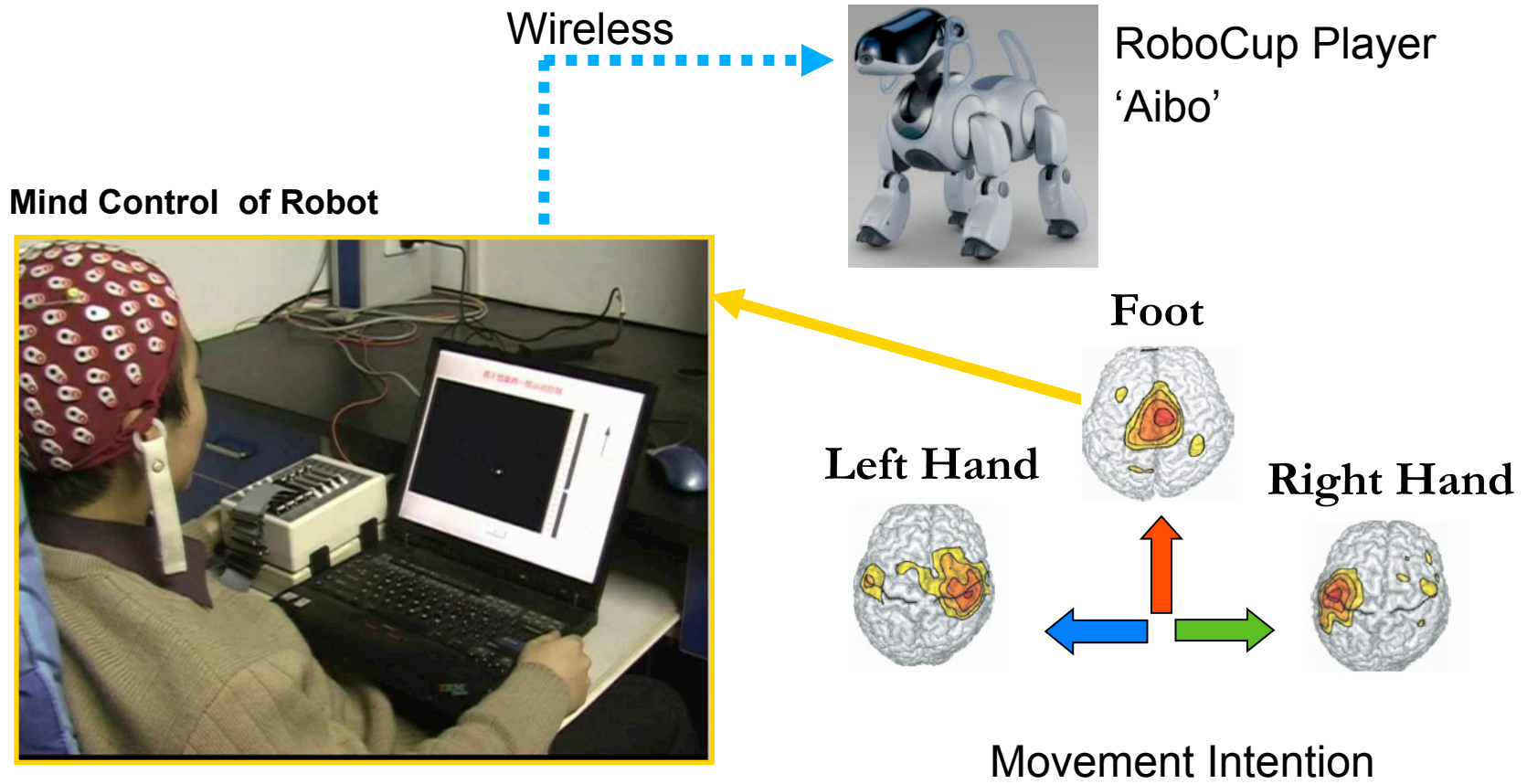
- P300 event-related potential BCI. (e.g. Donchin et al, *IEEE Trans Rehabil Eng* 2000.)
- Sensorimotor rhythm BCI.
- Steady-state Visual Evoked Potential.
- Time-frequency EEG features

P300 BCIs

- Farwell and Donchin 1988
- [P300 Speller](#)



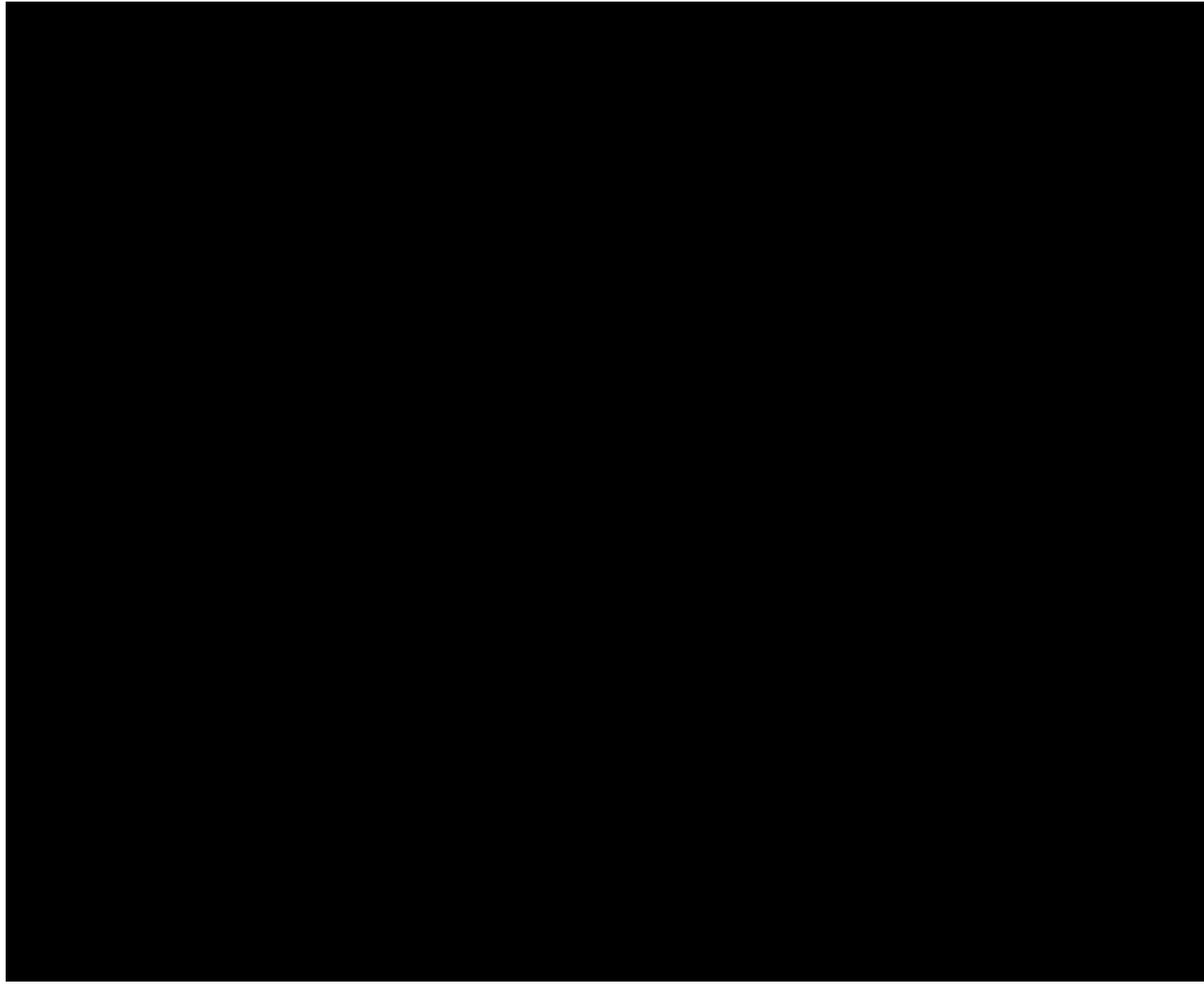
- Motor imagery BCI



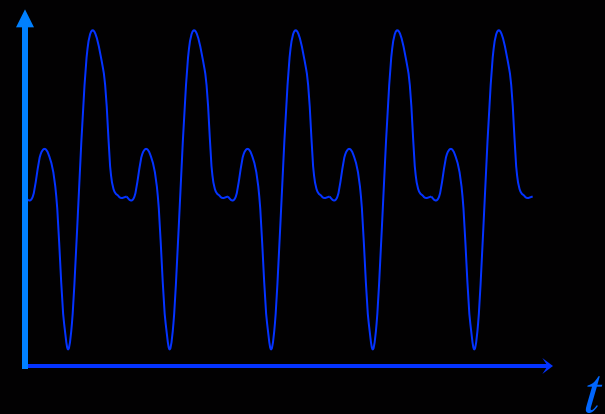
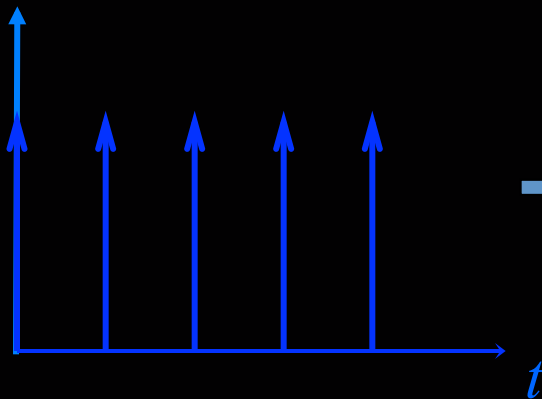
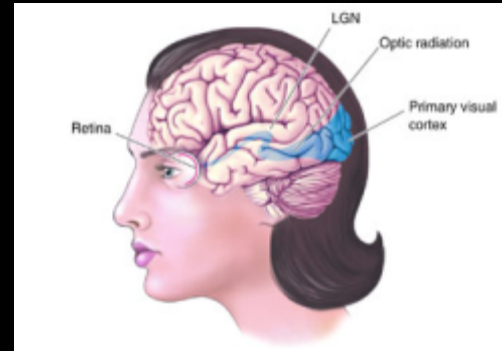
Mu BCIs



Mu BCIs



Reactive (SSVEP) BCIs



SSVEP BCIs

A Cell-Phone Based Mobile & Wireless Brain-Computer Interface

Yute Wang, Yijun Wang, Tzyy-Ping Jung
National Chiao-Tung University
University of California San Diego

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BioSig



- Developed at TU Graz since at least 2002
- One of the oldest open-source BCI toolboxes, for MATLAB/Octave (cross-platform)
- *Large amount of functionality* from statistics and time-series analysis: Adaptive Autoregression (AAR), Blind Source Separation (BSS), Common Spatial Patterns (CSP), Classifiers (LDA, SVMs, ...), Cross-Validation
- *Offline analysis only* -- no real-time hardware or computation support
- *Not easy to use* (no GUI, fairly complicated code, not very modular...)

BCI2000

- Developed at Wadsworth Center since 2000
- *Large, modularized C++ system*, primarily aimed at real-time acquisition, signal processing, stimulus presentation, experiment control, deployment; robust, “enterprise-grade” implementation (though Windows only)
- Supports a *wide range of acquisition hardware* (currently 19 systems)
- Solid documentation, workshops, book, big community
- *Lack of advanced signal processing and machine learning algorithms* (tough extensions and in-house versions available)

OpenViBE



- Developed at INRIA, relatively young project
- Implemented in modular C++, focusing on *visual programming and dataflow programming*
- *Very user-friendly design, interface and documentation*
- Focus on basic signal processing building blocks, weaker support for complex information flows (machine learning, adaptive signal processing, ...)
- Relatively hard to extend due to complex framework
- Supports a broad range of acquisition hardware (15 systems), runs on Windows and Linux

g.BSanalyze

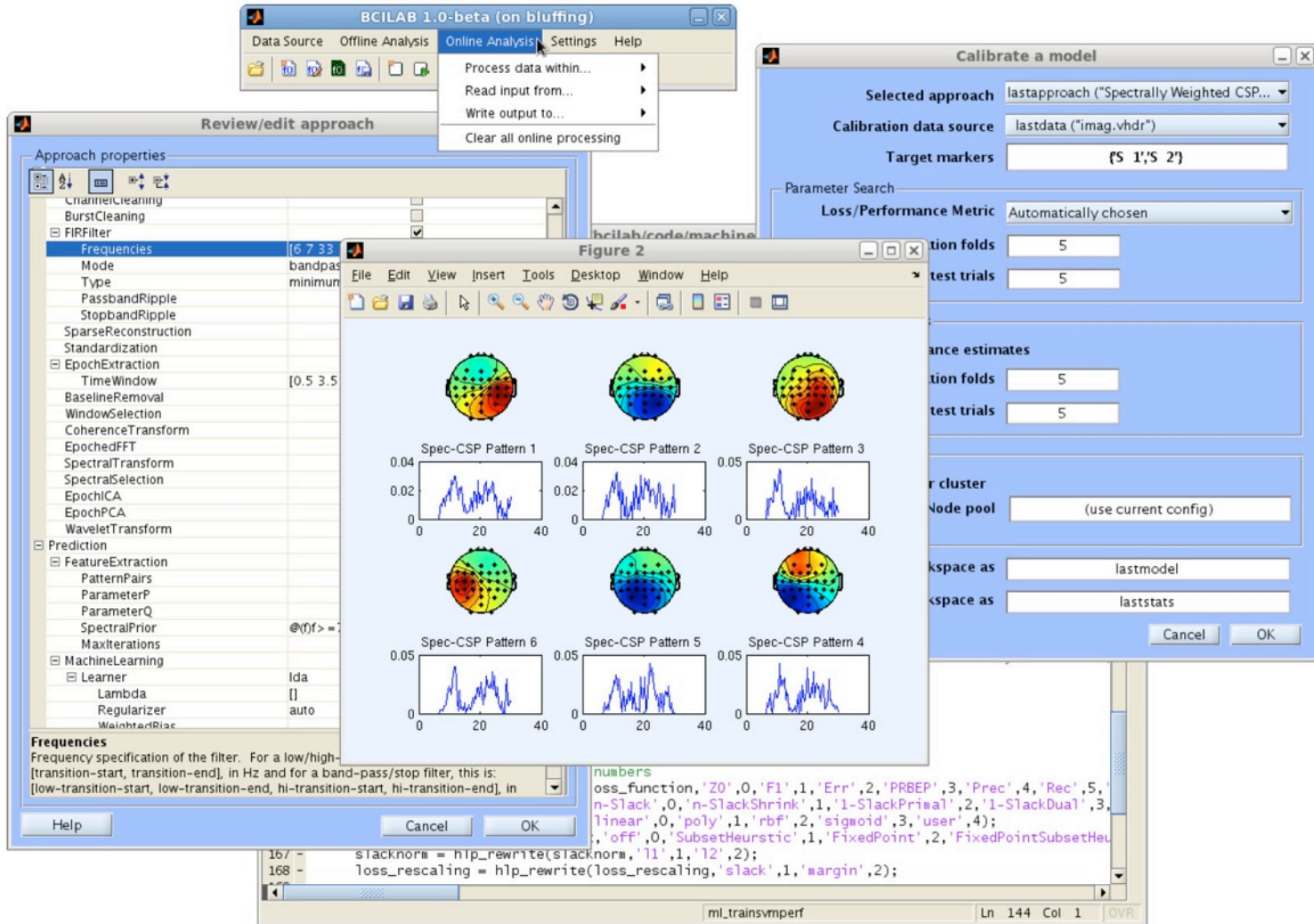
- Commercial System developed by g.Tec
- MATLAB/Simulink-based framework
- Broad collection of turnkey algorithms, evaluation methods, etc.
- Extensive, high-quality graphical user interface
- Primarily supporting in-house amplifiers



BCILAB

- Developed since 2010 at Swartz Center for Computational Neuroscience, UCSD (precursors dating back to 2006)
- MATLAB-based, cross-platform, offline and online analysis; stand-alone versions available
- *Largest collection of BCI algorithms* from signal processing, machine learning, etc.
- Relatively little native support for acquisition systems (5), but can tie into real-time experimentation frameworks (BCI2000, LSL)

BCILAB Sample GUI



The screenshot displays the BCILAB 1.0-beta GUI with several windows open:

- BCILAB 1.0-beta (on bluffing)**: The main application window with a menu bar (Data Source, Offline Analysis, Online Analysis, Settings, Help) and a toolbar.
- Review/edit approach**: A window showing approach properties and a list of processing steps such as ChannelCleaning, BurstCleaning, FIRFilter, Frequencies, and Prediction.
- Calibrate a model**: A dialog box for model calibration with fields for Selected approach, Calibration data source, Target markers, Loss/Performance Metric, and various fold and trial counts.
- Figure 2**: A window displaying six topographic maps and line plots labeled Spec-CSP Pattern 1 through 6, showing spatial and temporal patterns.
- Code Editor**: A window showing MATLAB code for training a support vector machine, including parameters like `loss_function`, `n-Slack`, and `stacknorm`.

<http://scn.ucsd.edu/wiki/BCILAB>
<ftp://scn.ucsd.edu/pub/bcilab>

From C. Kothe, BCILAB
Workshop Tutorials

Toolbox Organization

Framework

GUI / Scripting Interfaces

Approach
Definition

Online
Execution

Offline
Evaluation

Visualization

Plugins

Signal Processing

ICA

SSA

FIR

IIR

FFT

...

Machine Learning

LDA

QDA

DAL

GMM

SVM

...

BCI Paradigms

CSP

Spec-CSP

ERP

RSSD

...

Devices

TCP

OSC

BCI2000

...

Infrastructure

GUI
generation

cluster
computing

disk
caching

helper
functions

environment
services

Dependencies

CVX

BNT

EEGLAB

GUI utils

LIBSVM

GLMNET

...

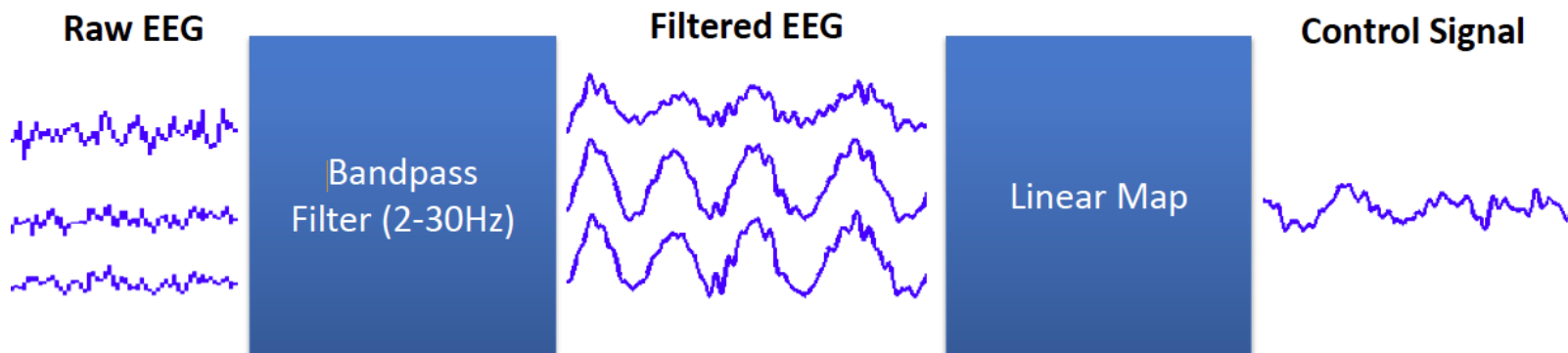
Driver
I/O

Other Packages

- **xBCI**: New C++ framework focused on online operation, GUI-centric, cross-platform
- **BF++**: Mature BCI framework (developed since 2000), however not very well known – mostly for offline analysis & modeling with UML and XML
- **TOBI**: Protocol suite for BCI interoperability and data acquisition
- **PyFF**: Python-based BCI stimulus presentation system
- **BBCI**: In-house MATLAB-based system developed at TU Berlin; very comprehensive, potentially for licensing
- **BCI++**: Relatively new C++ system, focused on human-computer interaction and virtual reality (still growing)

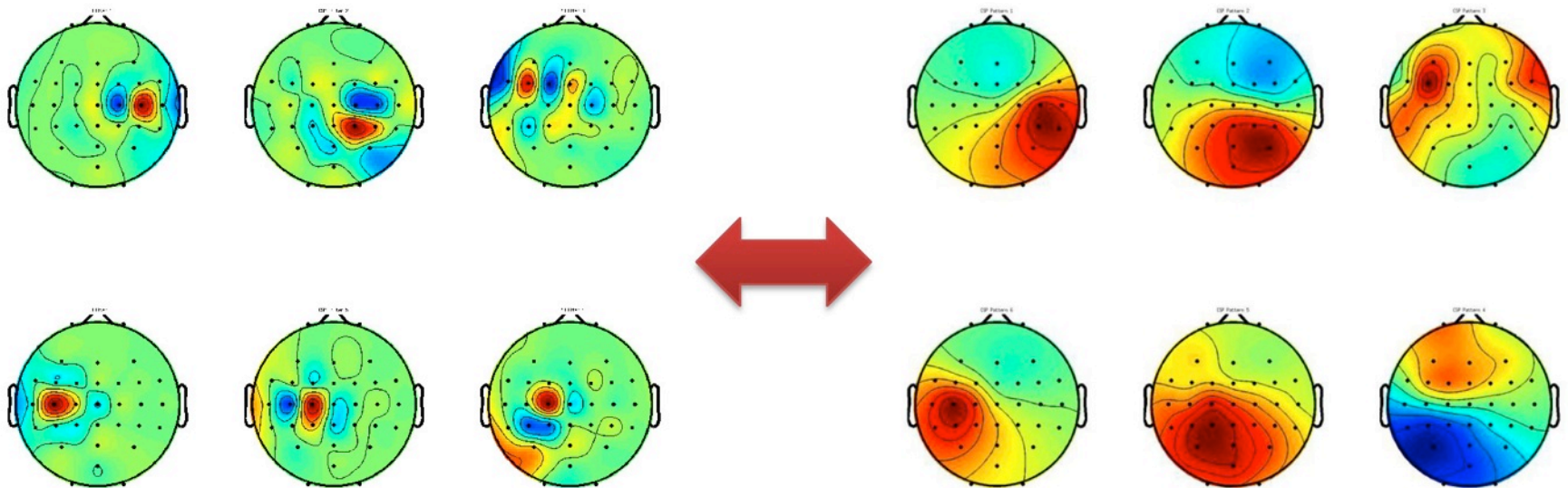
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- 1. Signal processing:** transforms one signal to another
- From the point of view of Signal Processing, a BCI transduces the input signal $x(n)$ (for example EEG) into a control signal $y(n)$
 - BCI components can be conveniently described as filters.
 - Relevant filter classes: Spatial Filters, Temporal Filters, Spectral Filters, Spatio-Temporal Filters, etc.



Spatial Filters vs. Forward Projections

- Spatial filters are *not* the same as forward projection maps of some source signal – they are the inverse operation



$$S(n) = \mathbf{W}X(n)$$

$$X(n) = \mathbf{W}^{-1}S(n)$$

Temporal Filters

- Transform a multi-channel signal $X(n)$ such that each channel $y_i(n)$ in $Y(n)$ depends only on the channel $x_i(n)$
- They are conceptually orthogonal to spatial filters
- Examples include time windowing, wavelet transform, etc.
- Special case: Spectral filters

Example Temporal Filters

- **Moving Average:**

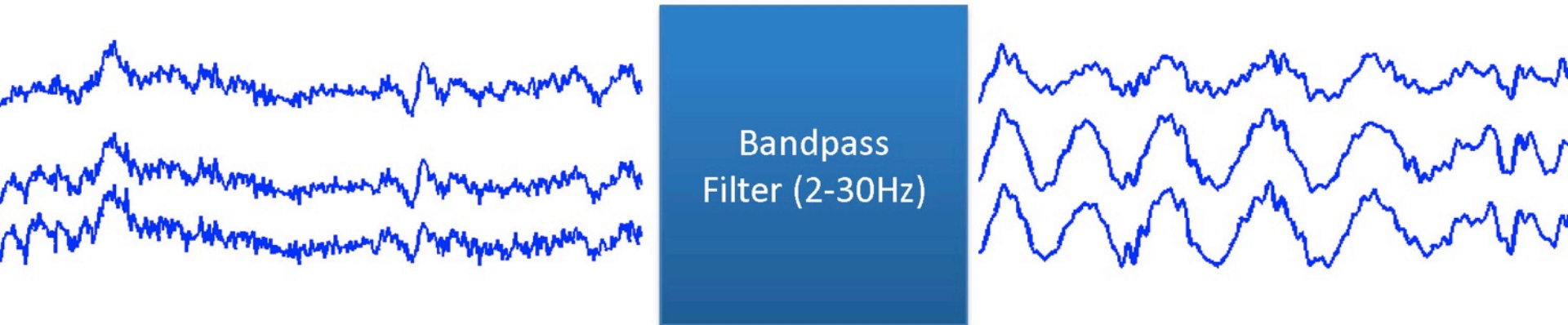
$$\mathcal{T} := y_i(n) = \frac{1}{m-1} \sum_{k=0}^m x_i(n-k)$$

- Effectively a smoothing (low-pass) operator
- In fact a simple example of a spectral filter



Spectral Filters

- Examples include: High-pass, Low-pass, Band-pass filters, Notch filters
- Their main utility in BCIs is to isolate oscillations or ERPs of interest



2. Feature Extraction:

Off-the-shelf machine learning methods often do not work very well when applied to raw signal segments of the calibration recording

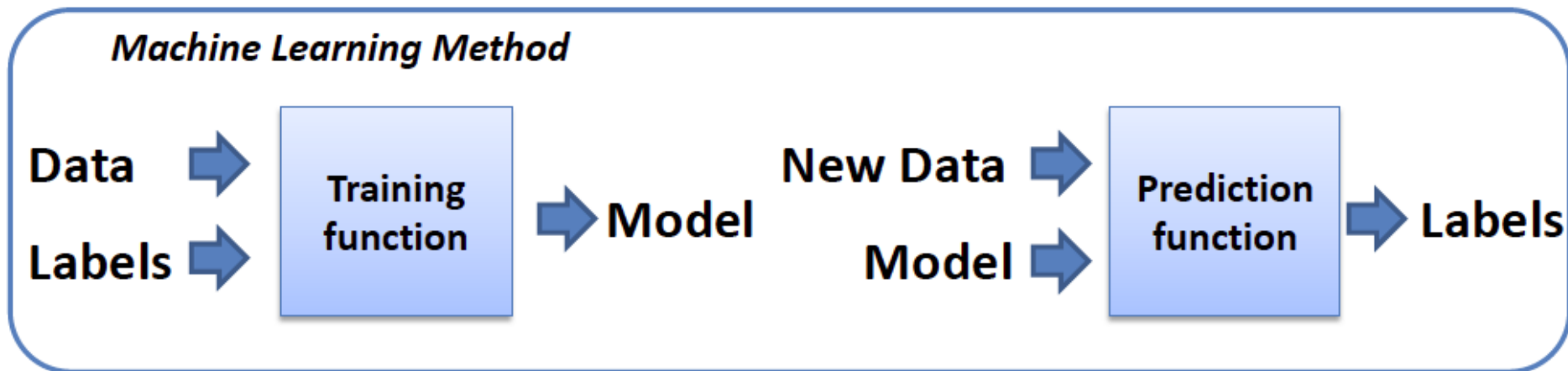
- too high-dimensional (too many parameters to fit)
- too complex structure to be captured (too much modeling freedom, requires domain-specific assumptions)

Typical Solution: Introduce additional mapping (called "feature extraction") from raw signal segments onto feature vectors which extracts the key features of a raw observations.

- output is usually of lower dimensionality
- hopefully statistically "better" distributed (easier to handle for machine learning).

3. Machine Learning

Most methods conform to a common framework of a training function and a prediction function



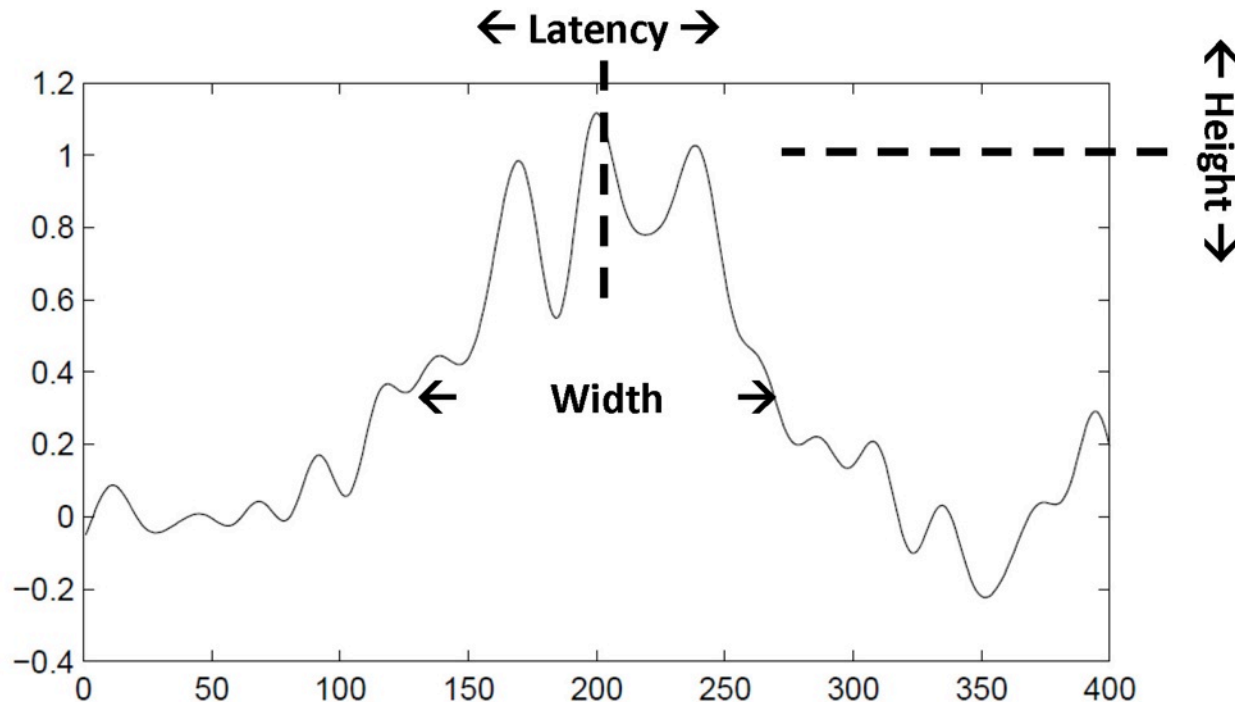
- **Supervised Learning:** given a set of (input,output) pairs as training data, learn a parametric (or “non-parametric”) model M that encodes the mapping from input to output
- **Unsupervised Learning:** given a set of training examples, learn the structure in the input space (e.g. clusters, manifolds, probability density)
- **Semi-Supervised Learning:** Some training examples have labels, others do not

Example Calibration Problem

- **Task:** A person is presented with a sequence of 300 images (one every 2 seconds). Half of the images are exciting, the other half are not. One channel of EEG (at Cz location) is recorded.
- **Question:** How to design a BCI that can determine whether a person is shown an exciting or a non-exciting image?
- **Approach:** For each trial k , cut out an epoch \mathbf{X}_k of 1s length, extract a short vector of features \mathbf{f}_k , and assign a label y_k in $\{E, NE\}$. Use machine learning to find an optimal statistical mapping from \mathbf{f}_k onto y_k .

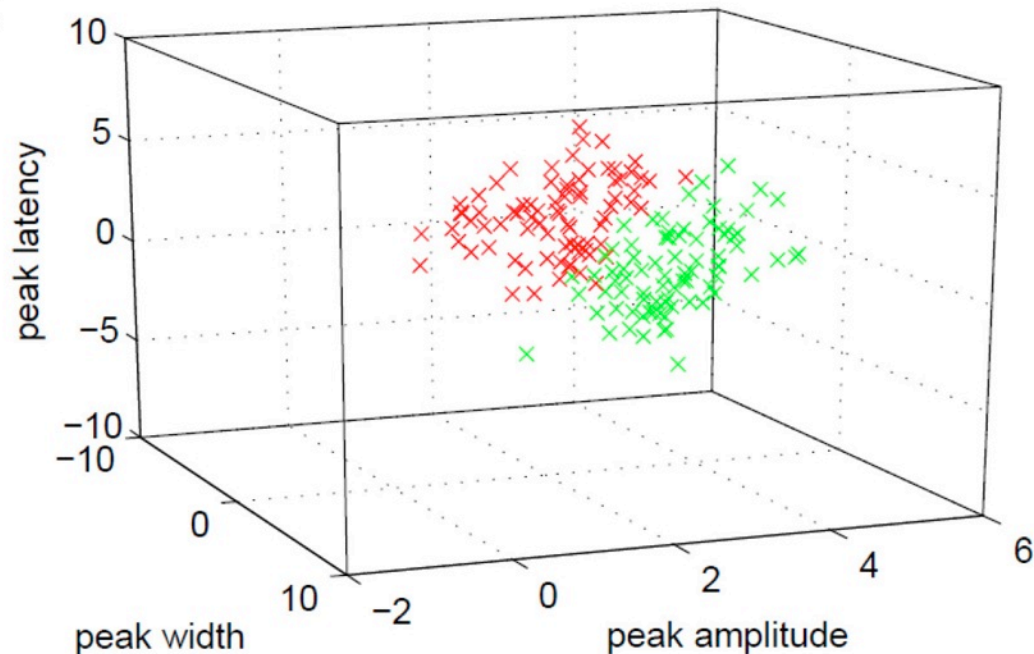
Extracting Features of a Peak

- A supposed characteristic peak in a time window (relative to an event) could be characterized by three parameters:



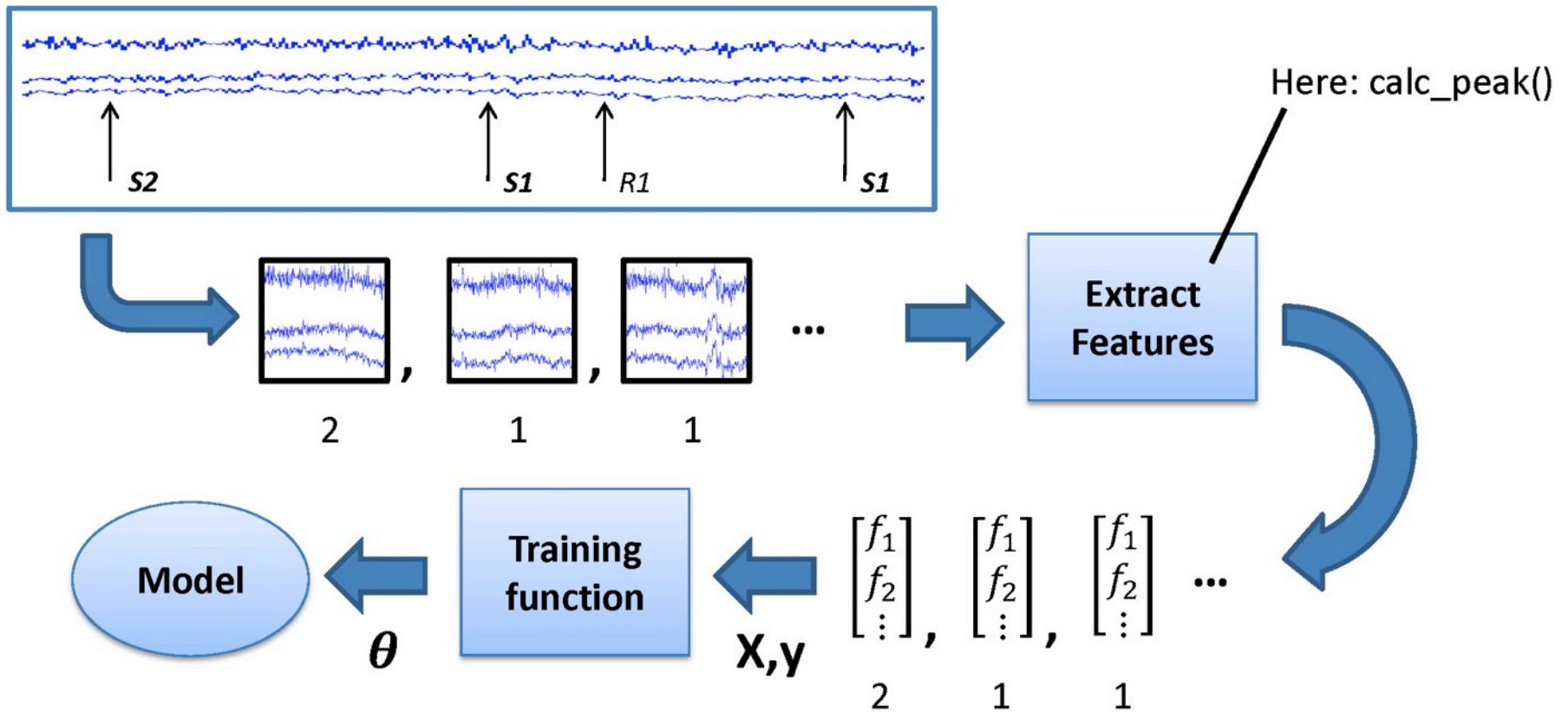
Resulting Feature Space

- Plotting the 3-element feature vectors for all exciting trials in red, and non-exciting trials in green, we obtain two distributions in a 3d space:



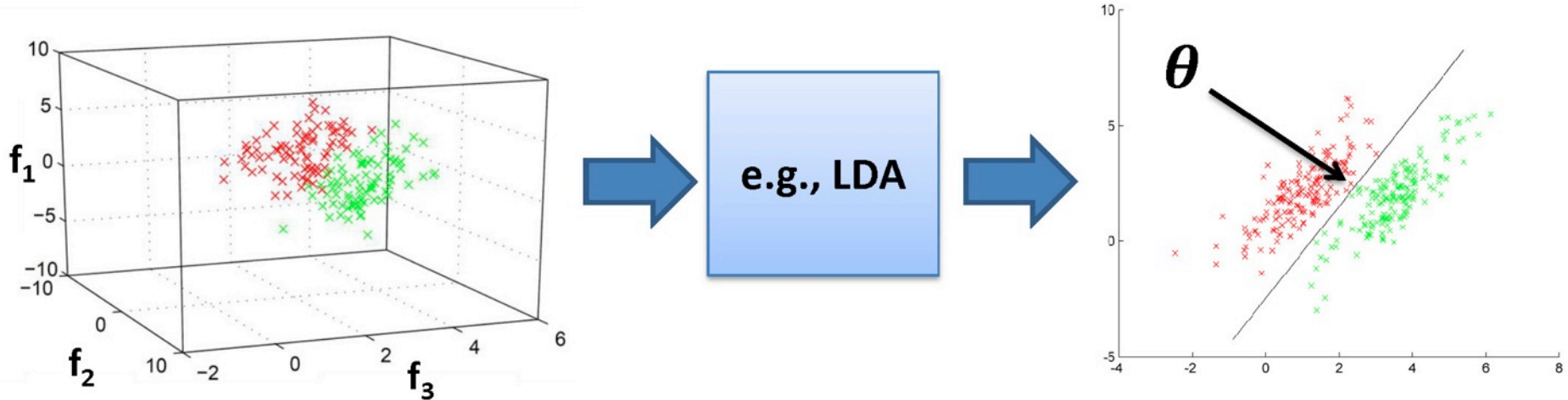
ML with Feature Extraction

- Including the feature extraction, the analysis process is as follows:



Using Machine Learning

- The feature vectors are passed on to a machine learning function (e.g., Linear Discriminant Analysis)
- ... which determines a parametric predictive mapping



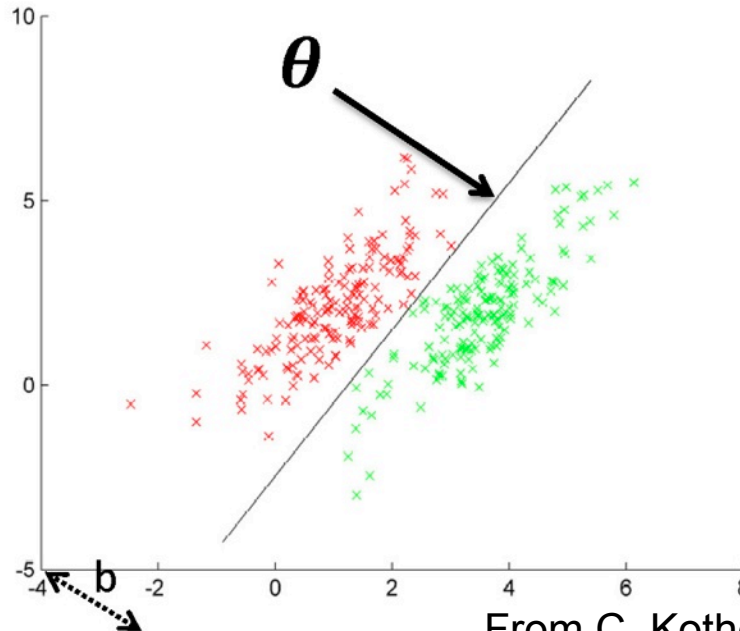
LDA generates parameters of a linear mapping: $y = \theta x - b$,
 For classification, the mapping is non-linear: $y = \text{sign}(\theta x - b)$.

LDA In a Nutshell

- Given trial segments \mathbf{x}_k (in vector form) in \mathcal{C}_1 and \mathcal{C}_2 ,

$$\boldsymbol{\mu}_i = \frac{1}{|\mathcal{C}_i|} \sum_{k \in \mathcal{C}_i} \mathbf{x}_k, \quad \boldsymbol{\Sigma}_i = \sum_{k \in \mathcal{C}_i} (\mathbf{x}_k - \boldsymbol{\mu}_i)(\mathbf{x}_k - \boldsymbol{\mu}_i)^\top$$

$$\boldsymbol{\theta} = (\boldsymbol{\Sigma}_1 + \boldsymbol{\Sigma}_2)^{-1}(\boldsymbol{\mu}_2 - \boldsymbol{\mu}_1), \quad \mathbf{b} = \boldsymbol{\theta}^\top(\boldsymbol{\mu}_1 + \boldsymbol{\mu}_2)/2$$



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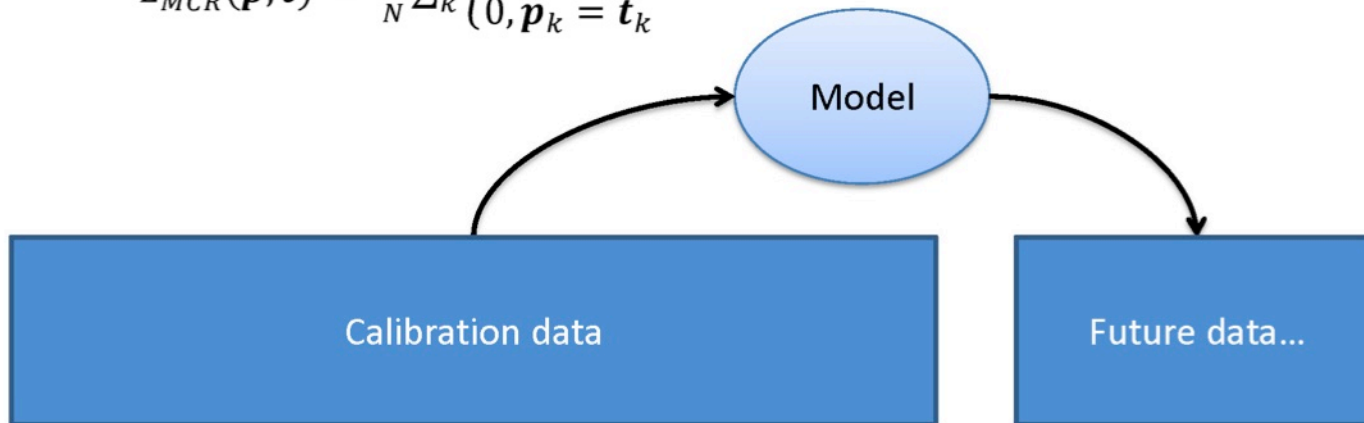
1. Both calibration data and test data are available
 - Estimate model parameters (for filters, features, ML algorithm)
 - Apply the model to new data (online / single-trial)
 - Measure prediction performance or loss between a vector of predictions \mathbf{p} and a vector of targets \mathbf{t} using, for instance,

- **Mean-Square Error:**

$$- L_{MSE}(\mathbf{p}, \mathbf{t}) = \frac{1}{N} \sum_k (\mathbf{p}_k - \mathbf{t}_k)^2$$

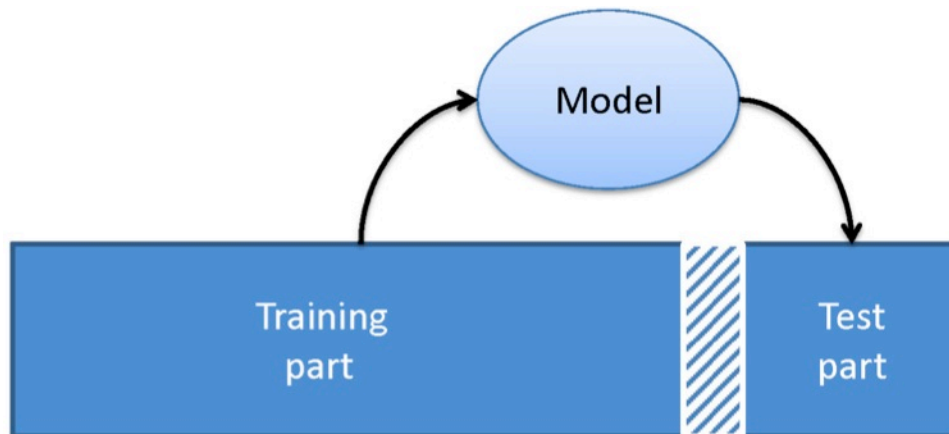
- **Mis-Classification Rate:**

$$- L_{MCR}(\mathbf{p}, \mathbf{t}) = \frac{1}{N} \sum_k \begin{cases} 1, & \mathbf{p}_k \neq \mathbf{t}_k \\ 0, & \mathbf{p}_k = \mathbf{t}_k \end{cases}$$



2. Test (future) data are not available

- Split one data set repeatedly into training/test blocks systematically, a.k.a. cross-validation
- Time series data: Prefer block-wise cross-validation over randomized
- Consideration: Since neighboring trials are more closely related than training and future online data, leave a margin of several trials/seconds between training and test
- Standard splitting schemes: 5x, 10x



3. Time (speed) matters

- Information Transfer rate (ITR)

$$B_t = \log_2 N + p \log_2 p + (1 - p) \log_2 \left[\frac{1 - p}{N - 1} \right]$$

N is the number of different types of mental tasks and the P the accuracy of classification.

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- Communication tool for severe disabilities such as tetraplegia, locked-in syndrome



P300 Speller

- Prosthetic control for severe disabilities such as tetraplegia, locked-in syndrome



KU Leuven



Brain2Robot
(Fraunhofer FIRST)

- Neurorehabilitation after neurological diseases or injuries



Takata et al., 2011



Gao, Wang et al.

- Entertainment and gaming



- Lie detection, Brain Fingerprinting, Trust assessment

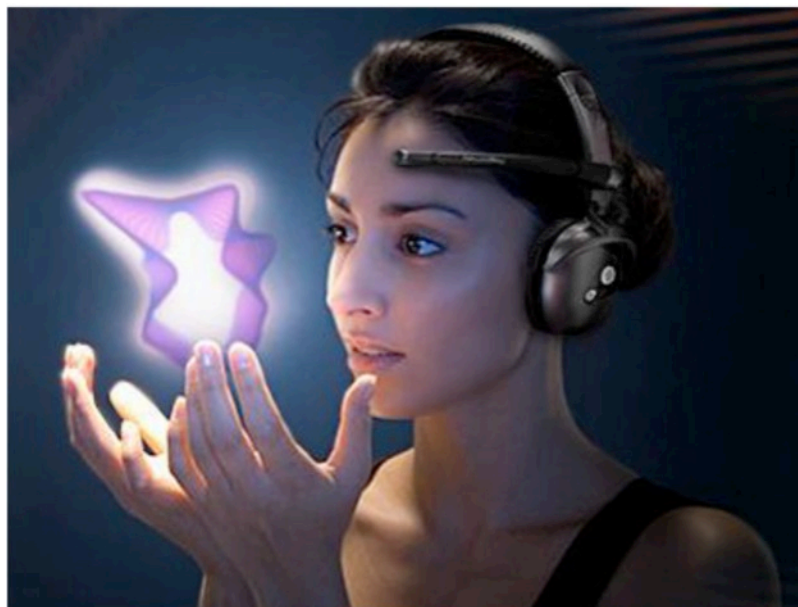


Farwell et al. 2000

- Health such as sleep-stage or mood monitoring

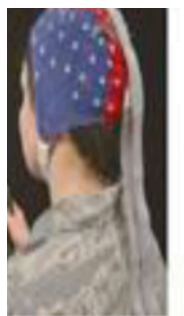


iBrain



Neurosky Mindset

- Cognitive-state, such as workload/fatigue/alertness, monitoring in pilots, air traffic controllers, plant operators



Pupil Diameter
Eye Blink Frequency
Cortisol Level in Saliva



Lin et al, 2008.



Haufe et al., 2011

- Ethical issues
- Acceptance by patient groups, etc.
- Difficult to prove their advantages over surrogate methods

- Signal-to-noise ratio of EEG is extremely low, especially in real-world environments,
- EEG signals are mathematically complicated to handle since all sensors record almost the same signal.
- Brain dynamics are very complex
 - Folding of cortex differs between any two persons
 - Relevant functional map differs across individuals
 - Sensor locations differ across recording sessions
 - Brain dynamics are non-stationary at all time scales
 - Brain dynamics are very variable across subjects, tasks, experimental conditions, etc.

- BCILAB tutorials and presentations: <ftp://sccn.ucsd.edu/pub/bcilab/>
- A. Bashashati, M. Fatourehchi, R. K. Ward, and G. E. Birch, "A survey of signal processing algorithms in brain-computer interfaces based on electrical brain signals", *J. Neural Eng.*, vol. 4, no. 2, pp. R32–R57, Jun. 2007.
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- R. Tomioka and K.-R. Mueller, "A regularized discriminative framework for EEG analysis with application to brain-computer interface", *NeuroImage*, vol. 49, no. 1, pp. 415–432, 2010.
- B. Blankertz, G. Dornhege, M. Krauledat, K.-R. Mueller, and G. Curio, "The non-invasive Berlin brain-computer interface: Fast acquisition of effective performance in untrained subjects", *NeuroImage*, vol. 37, no. 2, pp. 539–550, Aug. 2007.
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